

1 MOTOR CONTROL SYSTEM FOR ENDODONTIC HANDPIECE
2 PROVIDING DYNAMIC TORQUE LIMIT TRACKING OF SPECIFIC FILE FATIGUE
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4 CROSS-REFERENCE TO RELATED APPLICATION

5 This application claims priority from U.S. Provisional
6 Application Ser. No.: 60/413,087, filed September 24, 2002.
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8 BACKGROUND OF THE INVENTION

9 1. Field of the Invention

10 The present invention generally relates to a computerized
11 control system for the drive motor of a dental handpiece and, more
12 particularly, to such a control system for taking account of the
13 condition of cutting tools used in the handpiece.

14 2. Description of the Related Art

15 Dental handpieces are used in root canal work for
16 motorized driving of root canal files and other cutting implements.
17 The breaking of a root canal file is a serious event, particularly
18 where the broken end of the file may remain embedded in the root
19 canal of the tooth. File breakage, as currently understood, occurs
20 when torsional stress thresholds for a given instrument are
21 exceeded during its rotation in the tooth. Also contributing to
22 this instrument failure is the accumulation of cyclic fatigue as
23 this instrument rotates in root canals that are curved. Such
24 cyclic fatigue develops due to the tensile stretching that occurs
25 in this file on the outside of its curvature and the compression
26 that occurs on the inside curvature at that same location along the
27 file's length. This compression/tension event is magnified by the

1 rapid rotation of the instrument during root canal preparation
2 procedures, alternately stretching and compressing the file around
3 its circumference.

4 Numerous efforts have been made by innovators in the
5 field to limit file breakage primarily by measuring torque values
6 imparted to the file during root canal shaping procedures and to
7 take corrective steps, such as sounding an audible warning and/or
8 slowing, stopping or reversing the handpiece motor when a reference
9 level is reached. However, this torque limitation safety feature
10 does not take account of accumulated fatigue which may contribute
11 to a reduction of permissible torque limit for a given instrument,
12 or the curvature of the root canal being shaped, thus resulting in
13 actual breakage. Neither does it account for the variations in
14 structural characteristics of the different shaping files used to
15 prepare a root canal.

16 A number of examples of such efforts from the prior art
17 are set out in the following.

18 Patent 4,243,388 of Arai discloses a dental hand engine
19 for driving a reamer for root canals. The disclosed system
20 incorporates a control device which electrically senses when the
21 forward end of the reamer reaches the radical apex of a tooth root
22 canal so that the engine and its reamer may be automatically
23 stopped.

24 Patent 4,955,810 of Levy discloses apparatus and method
25 for measuring thickness of the dentin layer of a patient's tooth.
26 In the disclosed process, the resistance to electrical current flow
27 from a voltage applied between the dentin and a spaced apart region

1 of the patient's body is used to indicate the thickness of the
2 dentin layer. Patent 5,538,423 of Coss et al. discloses a dental
3 drilling system having a programmable control unit for controlling
4 operating parameters of the drilling system, such as direction of
5 rotation, speed of rotation, torque of the dental drill tool bit,
6 pumped irrigation fluid flow rate, and the intensity of light from
7 a light source, to name a few. The control unit may be programmed
8 with sets of data values representing a desired value for each of
9 the operating parameters to be controlled. The system is said to
10 accurately achieve and maintain a specified rotation speed or
11 torque.

12 Patent 4,723,911 of Kurtz discloses apparatus for high-
13 speed drilling of bone tissue of varying density to produce
14 proportioned variations in the speed of the drill. Instantaneous
15 bur rotational speed is automatically sensed to produce a signal
16 representing a change in speed, correlating to an indication of the
17 density of the bone tissue.

18 A number of systems for controlling motor speed or other
19 parameters of a drill system outside the field of endodontics are
20 known. For example, patent 5,038,084 of Wing describes a closed
21 loop control system which senses the current of a drill motor in
22 order to cause the drill motor to slow down as current decreases,
23 such as when the drill cuts through a workpiece.

24 Patent 5,543,695 of Culp et al. discloses a powered
25 medical instrument including a manually operable foot switch for a
26 motor control unit coupled to an autoclavable handpiece. In
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1 operation, a maximum torque value is set for a control circuit
2 which limits the motor torque to the selected value.

3 Patent 5,116,168 of Aihara discloses a control system for
4 a machine drill making holes through a composite workpiece made of
5 materials having different machining properties. Sensors detect
6 feed speed and rotational speed, respectively, as well as thrust
7 force applied to the drill. The resulting sensor signals are
8 compared with optimum values to control the feed speed and
9 rotational speed of the drill.

10 Patent 4,822,215 of Alexander discloses an automatic
11 drill system which also utilizes thrust and torque sensors for
12 enabling a computer to control the drill for an efficient drilling
13 operation for laminated materials, a non-dental application.

14 Patent 5,980,248 of Kusakabe et al. discloses a motor
15 controller for a dental handpiece which uses signals from a torque
16 sensor which detects the load torque applied to the cutting tool to
17 either stop the drive motor, reduce the rotational speed thereof or
18 temporarily reverse motor direction when the detected load torque
19 has reached a preset reference value. This system is said to
20 prevent a cutting tool, such as a relatively slender file for root
21 canal formation, from breaking during the procedure.

22 The breaking of a root canal file with the broken-off
23 part remaining in the tooth undergoing treatment represents
24 somewhat of a disaster. Any system which relies on the sensing of
25 drive motor torque or file tip position and comparing the read-out
26 signals with preset reference levels is still subject to failure
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1 (i.e., file breakage) when the reference levels are not set
2 properly.

3 Unexpected file breakage in a system in which the torque
4 or other parameter sensors are functioning properly and the preset
5 reference levels are within normal limits can still occur in
6 instances where the file itself may have developed fatigue from
7 repeated use in the standard endodontic procedure so that its
8 likelihood of breakage is no longer governed by the statistical
9 data applicable to a standard population of unused files.

10 Unexpected file breakage can also be caused by obvious
11 and hidden canal curvatures. Canal curvatures which introduce
12 fatigue to files range from even slight coronal curvatures to
13 severe apical curvatures. Furthermore, molar root canal curvatures
14 are always multiple in number and multiplanar in direction.
15 Endodontic shaping files are subject to cyclic fatigue when
16 curvatures are significant, even when the canal is relatively large
17 and little torsional stress is imparted to its fatigue history.
18 Even the largest file diameters will break when challenged by
19 cyclic fatigue.

20 Fatigue in any drilling implement is difficult to
21 determine. Therefore it is difficult to predict whether a given
22 drill will perform satisfactorily in a control system where the
23 reference limit values are standard and where the sensors for
24 measuring torque or other parameters are performing properly.

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1 SUMMARY OF THE INVENTION

2 In brief, arrangements in accordance with the present
3 invention involve a system which measures operating parameters
4 relating to the fatigue factor in a drill so that the drill may be
5 discarded or the rotational speed and/or torque limits be
6 dynamically reduced in proportion to the accumulated fatigue at
7 some point in the repetitive use cycle where the predicted fatigue
8 level in the drill warrants discontinuing any further use at the
9 most basic level. This handpiece system records the total number
10 of revolutions each individual file has turned, as well as the
11 torsional stresses accumulated during those revolutions. It may
12 also keep track of other operating factors which bear on
13 accumulated fatigue such as, for example, the direction of
14 rotation, the speed of rotation, and the torque at the file tip, as
15 well as the size and taper of the file being used. It keeps track
16 of this data on an individual file basis, displaying the data as
17 desired when a file is selected for re-use (after sterilization)
18 and using it to provide an appropriate torque limit for the
19 starting point for the next period of use.

20 In accordance with one aspect of the invention, provision
21 is made for storing individual files in autoclavable file storage
22 boxes. An operative connection is established between the storage
23 boxes and the control system computer to provide a display of the
24 data history of a given file upon command. In this manner, the
25 professional is able to match a given file to the anticipated usage
26 for a particular task. In simple terms, if a short duration
27 drilling task is encountered, a drill may be selected which already

1 has a significant fatigue data history, and the control system
2 could drive the drill at speeds and torques which are below the
3 predicted limits of breakage for that particular drill. On the
4 other hand, such a drill would be avoided if the task to be
5 performed is likely to involve higher levels of stress which might
6 be more likely to result in breakage during the anticipated task.

7 Another method of use would be for this device to simply
8 indicate when individual files in a sterilization organizer box
9 should be replaced. In accordance with this aspect, a method is
10 disclosed by which the system microprocessor can keep track of many
11 individual files and many different file sets in the doctor's
12 office. As it is now, whole sets of instruments are discarded
13 after one procedure in an attempt to err on the careful side, by
14 using fresh files at the start of every case. This is much better
15 than the risky process of using the same file in a certain number
16 of canals which requires careful marking on used files and it only
17 counts the number of canals cut; this is not safe enough. While
18 using new files greatly reduces possible error, it also causes
19 inadvertent profligacy. In the interests of safety, many files are
20 prematurely discarded. Conversely, 20-.10 files last much longer
21 than 20-.06's for instance. Small new files could still be broken
22 when a second new file should be brought in before the end of that
23 procedure.

24 Another critical factor, after the design and fatigue
25 history of instruments, is the canal curvatures through which the
26 instruments will be required to work. The procedurally important
27 variations of canal curvature are the location of curvature, the

1 radius of curvature, and finally, the degree of curvature. With
2 that said, each root canal often has multiple curvatures, each of
3 them again has a different location, acuity, and degree of
4 curvature. The fact that many of these curvatures are hidden in
5 clinical radiographs further challenges the clinician in preventing
6 file breakage.

7 Systems of the invention may also include a testing model
8 which will consistently replicate specific root canal dimensions
9 and curvatures in dentin and synthetic materials so that many of
10 the same size and geometry of specific endodontic instruments can
11 be tested to failure in many identical and anatomically correct
12 root canal test models, thereby allowing greater predictability in
13 the anticipation of future failures of those same files in clinical
14 practice. In accordance with this aspect, a method is disclosed by
15 which the system microprocessor can keep track of many individual
16 files and many different file sets in the doctor's office.

17 Fatigue in a dental drill develops as a function of the
18 number of occasions and length of time when the stress applied with
19 a given parameter has exceeded the elastic limit for that
20 parameter, thereby incurring a change, however slight and
21 undetectable, in drill quality. This introduces fatigue such that,
22 if operation of the drill is continued, the risk of breakage may be
23 significantly increased. The specific figures for the elastic
24 limits to be taken into account in tracking the accumulated fatigue
25 for a given dental drill may be provided by the manufacturer of the
26 drill. However, manufacturing testing seldom matches clinical
27 conditions. Also what is needed to be recorded is the number of

1 times a given torque limit was hit or approached, also the duration
2 at the limit and the torque value as well as the number of
3 rotations. If not so provided, they may be determined empirically
4 by testing to destruction of sample drills of a type and set in
5 accordance with an aspect of the invention disclosed above. The
6 result will be an increase in the confidence level that a given
7 drill may be used with reduced likelihood of breakage.

8 Each of the parameters which are understood to contribute
9 to accumulated fatigue during use of a given drill may have a
10 determinable strain limit which can be used in operating a control
11 system to prevent a given drill from reaching its fatigue limit.
12 Operating a drill with such a control system not only significantly
13 reduces the extent of drill breakage in performing root canal work
14 on a tooth, but it serves to prolong drill life, allowing repeated
15 use of a particular drill with safety and confidence that repeated
16 use of the drill is justified.

17 All of the capabilities of the system to predict file
18 breakage are incumbent upon correctly modeling the fatigue curve
19 for each type and size of instrument as they shape different root
20 canal morphologies. Heretofore there has been no known method that
21 could simulate specific root canal anatomy and accurately replicate
22 the stresses placed on files in that environment. Extracted teeth
23 have traditionally been used to test prototype instruments as well
24 as to teach dentists the use of new instruments and techniques;
25 however, they are limited in their use in determining fatigue
26 curves due to the virtually infinite variability of natural root
27 canals.

1 Testing and teaching has also been done in the field with
2 epoxy-resin root canal models which can be made with reproducible
3 diameters and curvatures. However, all of the artificial materials
4 used to date behave very differently from the dentin encountered in
5 root canals, specifically by softening in the presence of heat
6 caused by cutting activity as well as by lacking the "lubricity" of
7 dentin, thus severely limiting the accuracy of data recovered.

8 One particular embodiment of the invention involves a
9 bovine dentin model that answers all of these problems. Because
10 cow molars are much larger than human teeth, several slabs of
11 bovine dentin can be sliced off each cow tooth. These are then
12 each milled flat on one side so that two of them may be clamped
13 together after several simulated root canals are cut into each
14 half. The canal halves are routed out of the bovine dentin blocks
15 with a computer-numerically-controlled milling machine so that
16 canal contours can be accurately reproduced in the block-halves.

17 With this machine technology, literally any canal
18 morphology a researcher wants to test files in could be cut in the
19 block-halves, either by manual design (dialing in diameters,
20 tapers, and curvatures) or better by using computer models of
21 canals reconstructed from microCT scans of extracted teeth. Most
22 important in research terms is the exact reproducibility of these
23 models, thereby increasing the accuracy of the predictive research
24 and application of the fatigue curve for each of the instruments
25 in all of the classic anatomic challenges presented by root canal
26 systems. In this method the morphologies of different canals are
27 subtracted from the computer reconstruction of the tooth, laid out

1 as curvatures in two dimensions, programmed into the CNC machine,
2 and the canal is cut into the two block-halves exactly as it was in
3 the original tooth. Another method is to cut the canal halves with
4 a CNC laser.

5 A final embodiment that also solves all current problems
6 with modeling file behavior in canals involves using
7 stereolithography to create anatomically correct models of roots
8 and root canals. In this method the computer model of the
9 reconstructed tooth is input to the system, directing a laser beam
10 to photo-polymerize successive layers of the model. The lubricity
11 of the dentin is replicated by mixing either collagen matrix
12 reconstituted from dentin or synthetic fibers with similar
13 lubricity into the photo-polymerized solution. The advantages of
14 this method over the bovine test model is the ability to reproduce
15 classic dental morphology quickly and relatively cheaply, with
16 virtually perfect anatomic accuracy, while maintaining adequate
17 functional characteristics such as dentin hardness and lubricity.

18 Whether the model is bovine dentin or resin, by testing
19 each file type and size to failure repeatedly in specific,
20 reproducible canal forms, a very accurate fatigue curve can be
21 drawn for that instrument operating in that type of canal.
22 However, a variable still remaining is a way to accurately assess
23 the amount of curvature in a canal, since so many canals have
24 curvatures hidden in normal views of dental x-rays. Another
25 embodiment of the invention is an instrument to "read" the curves
26 in a patient's root canals. After a root canal has been negotiated
27 and enlarged to a 15-.02 K-file size, a non-cutting file probe is

1 placed into the handpiece, the curve measurement function is
2 switched on the handpiece control, and the probe is taken to length
3 in the canal. The controller measures the torsional resistance to
4 rotation of the smooth-sided probe in the canal and factors that
5 into the torsional stress history of each file used in that canal
6 so that a more accurate estimate may be made of when the fatigue
7 curve for that file has gone into dangerous territory. The same
8 probes are spun in each of the simulated canal models the files are
9 tested in, so that each of the fatigue curves generated can be
10 related to a specific amount of canal curvature. Then, when the
11 clinician uses the curvature probe to measure the curves of the
12 canal to be shaped, the computer can choose the correct fatigue
13 curve in predicting failure of that file in that canal.

14 With individual file data collected and correlated with
15 corresponding files through the procedures described above, it may
16 be expected that the use of systems in accordance with the present
17 invention will not only make it possible for the professional to
18 perform his or her task with significantly reduced risk of file
19 breakage under circumstances which may adversely affect the
20 patient, but the cost of the files used by the professional over a
21 given period of time will be significantly reduced.

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23 BRIEF DESCRIPTION OF THE DRAWINGS

24 A better understanding of the present invention may be
25 realized from a consideration of the following detailed
26 description, taken in conjunction with the accompanying drawings,
27 in which:

1 FIG. 1 is a schematic block diagram of a first portion of
2 one particular arrangement in accordance with the invention;

3 FIG. 2 is a schematic block diagram of a second portion
4 of the system of the invention;

5 FIG. 3 is a schematic drawing of a two-part block
6 encasing a simulated root canal;

7 FIG. 4 is a schematic drawing of one of the parts of the
8 block shown in FIG. 3;

9 FIG. 5 is a schematic block diagram of a file
10 organization box with sensors at each file location and a
11 communications link that plugs into a handpiece control unit;

12 FIG. 6 is a schematic block diagram illustrating a stereo
13 lithographic process applicable to systems of the invention; and

14 FIG. 7 shows a smooth root canal probe which is used
15 prior to shaping the canal to measure obvious and hidden root canal
16 curvatures.

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18 DESCRIPTION OF THE PREFERRED EMBODIMENTS

19 FIGS. 1 and 2 together illustrate a system 10 comprising
20 a data collection portion 10A (FIG. 1) and a file selector portion
21 10B (FIG. 2).

22 The data collection portion 10A is shown comprising a
23 handpiece 12 having a file 14 installed therein. The handpiece 12
24 is controlled in its operation by a control stage 16 which operates
25 in response to signals from a computer 18 over a connecting line
26 20. Computer 18 is equipped in conventional fashion with a display
27 device 22 and one or more input devices 24 which may be a keyboard

1 26, a mouse 28, a foot control 30 and/or other similar devices such
2 as a trackball, a touchscreen, a touchpad, and the like.

3 The data collection portion 10A also includes a number of
4 sensors, such as a speed sensor 50, a torque sensor 52, a threshold
5 counter 54 and one or more sensors 56 to keep track of other
6 parameters relating to the handpiece tool 12. Each of these
7 sensors receives as its input corresponding outputs from the
8 handpiece tool 12. Each sensor 50, 52, 54, 56, converts its input
9 from the handpiece tool 12 into signals which are appropriate for
10 the processing and ultimate collection as data in a computer 18.
11 They may be applied directly to the computer 18 or, if desired,
12 they may be processed in a weighting stage 60 and an integrator 62
13 before being stored in the computer 18. The file selection portion
14 of FIG. 10B is shown as comprising a computer 18', which may be the
15 computer 18 of FIG. 1, coupled to a file records stage 70 where
16 records corresponding to the individual files are stored for
17 selection in the file selection portion 10B. The file selection
18 portion further includes a file storage member 72, a location
19 marker stage 74 which is connected between the file storage member
20 72 and the computer 18', and a stage 76 for selecting and
21 delivering a file such as 14 from the file storage member 72. In
22 one embodiment the file storage member 72 is an autoclavable box
23 having a plurality of slots or pockets for receiving individual
24 files for reuse.

25 In operation of the system 10, a number of endodontic
26 files are provided with unique identification codes. These unique
27 codes are entered into the computer 18, together with data

1 regarding the various file parameters, such as file type, file
2 size, and the like. If the files have been used, the individual
3 file records also contain the data derived by way of the sensors of
4 FIG. 1 from the operation of the file 14 and the handpiece 12.
5 These files are placed in the file storage box 72 with their
6 individual locations noted by the location marker 74 and stored as
7 part of the record in the computer 18'. When the professional
8 needs to select a file for a particular root canal preparation, he
9 enters the desired parameters into the computer and the computer
10 monitor displays the data of, for example, five particular files
11 which are in the storage box 72. The professional may select one
12 of the files presently displayed (using the cursor and the ENTER
13 key) or he may cause the computer to bring up another five files
14 for display on the monitor. As an alternative option, the
15 professional may plug in the file box and simply select from files
16 in the "used" section until they slow down to uselessness and are
17 replaced with the "reset" button being pushed. Once a particular
18 file is selected, it can be retrieved manually or the retrieval
19 mechanism of the select and deliver stage 76 can be used to
20 retrieve the file from the storage box and deliver it to the dental
21 office site.

22 In the operation of the preferred embodiment, each dental
23 office will have a number of endodontic file boxes, each with
24 identification numbers. Each specific file location in each
25 specific file box is coded. These file boxes are specifically
26 designed for each of the file systems available so that a file
27 storage tube exists, and is labeled for each file geometry in that

1 specific shaping system. When a file is selected for use the
2 sensor adjacent to the now-empty file tube signals as such to the
3 handpiece computer. The computer knows the fatigue curve of that
4 file geometry and manufacturer, the fatigue history of that
5 specific file, and the canal curvatures and locations of said
6 curvature.

7 Alternatively, each file could have a unique ID number on
8 it, said ID number tracking any of a number of methods, including
9 but not limited to bar codes, magnetic code, subtle shank geometry
10 codes. When the dentist needs another file, he or she keys the box
11 and specific file code into the handpiece control unit, or simply
12 by pulling out the file from the box, the handpiece control
13 computer knows which file is being used.

14 In this system, when a file is selected for use, the
15 computer looks at accumulated cycles and torque values and sets a
16 dynamic torque limit appropriate for that file geometry and that
17 file's history of use, and the canal curves in the canal to be
18 shaped. At a threshold point the file is discarded because the
19 handpiece controller display says so or because the dynamic torque
20 limit is too low to cut effectively.

21 FIGS. 3 and 4 illustrate a block containing sections of
22 a cow's tooth prepared for use with the system of the invention.
23 In FIG. 3, a block 80 is shown comprising two half-blocks 82, 83.
24 Slabs 84, 85 represent sections taken from a cow's tooth.

25 In FIG. 4, the half-block 82 is shown containing the slab
26 84 of a sectioned cow's tooth. In the slab 84, a plurality of root
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1 canals 86 have been cut in accordance with the methods described
2 herein.

3 FIG. 5 is a schematic block diagram of a file box and
4 hand control unit comprising a second embodiment in accordance with
5 the invention. FIG. 5 depicts a file storage box 100 partially
6 broken away to show a plurality of file storage compartments 102,
7 each provided with a sensor 104 and a file ejector 108. The
8 sensors 104 are individually connected to a cable 105 in a link 110
9 to feed file identification signals to a hand held control member
10 112. In conventional fashion, similar to a cell phone, the control
11 member 112 is provided with a display 114 and control buttons 116,
12 including RESET and ENTER buttons; up, down and side movement
13 arrows; and any other appropriate mode control selectors. The
14 ejectors 108 are individually connected to a cable 109 also
15 contained with the cable 105 in the connecting link 110 to the hand
16 held device. Instead of the wired link 110, the link to the hand
17 held device 112 may be an optical link 110A, or a wireless link.

18 In the operation of the embodiment of FIG. 5, each file
19 (not shown) is coded with an identification code. This code may
20 contain all of the relevant data for that specific file. When the
21 dentist needs another file, he may simply pull a file out of the
22 box or he may key into the hand-held control box 112 the data
23 representing the parameters of the type of file he is looking for,
24 using the buttons 116 in matching data from acceptable files which
25 are sensed by the sensors 102 as the data appear on the display
26 114. Selection may then be made by the appropriate buttons 116 and
27 an appropriate ejector 108 may be energized by pressing a return

1 button on the control member 112. The file is then made available
2 for selection or for insertion into the dental handpiece.

3 FIG. 6 represents, in block diagram form, a process of
4 stereolithography which may be useful in the practice of the
5 present invention. Block A of FIG. 6 represents the first step in
6 the process, which involves a Micro CT scan of an extracted tooth.
7 Block B represents a 3-dimensional reconstruction to extract inner
8 and outer surface dimensions and generate a stereolithography data
9 record. This is followed by Block C representing the step of a 3-
10 dimensional rapid prototyping machine creating a physical model of
11 a tooth from the established data. The result is shown in Block D
12 as a duplicate model of the original extracted tooth, including the
13 interior anatomy.

14 FIG. 7 is a schematic representation of a tooth in cross-
15 section, with a probe device 120 comprising a handle 122 and a
16 long, thin probe member 124. The member 124 is inserted into the
17 root to the distal end, and is used by the professional to
18 determine the extent of the root canal.

19 In the practice of embodiments of the invention, it
20 becomes possible to reuse particular files with confidence that the
21 file is safe to use. The computer keeps track of the prior uses of
22 the file, specifically the number of revolutions and the
23 accumulated torsional stresses encountered by the file in previous
24 use, and records this as a cumulative stress history of the file.
25 With this cumulative history, the likelihood of file breakage under
26 specific conditions can be predicted and avoided.

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1 Although there have been described hereinabove various
2 specific arrangements of a MOTOR CONTROL SYSTEM FOR ENDODONTIC
3 HANDPIECE PROVIDING DYNAMIC TORQUE LIMIT TRACKING OF SPECIFIC FILE
4 FATIGUE in accordance with the invention for the purpose of
5 illustrating the manner in which the invention may be used to
6 advantage, it will be appreciated that the invention is not limited
7 thereto. Accordingly, any and all modifications, variations or
8 equivalent arrangements which may occur to those skilled in the art
9 should be considered to be within the scope of the invention as
10 defined in the annexed claims.

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